

Tissue Optical Properties

Indirect Measurements in Bulk Tissue

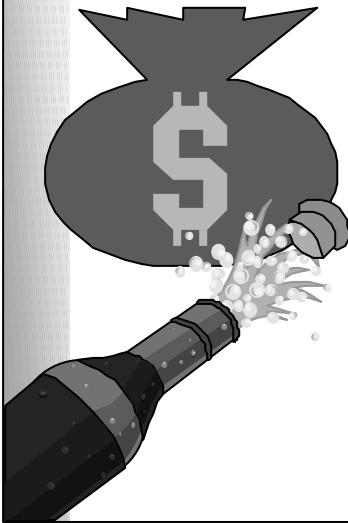
Medical Optics

Evaluation with diffusion theory

Indirect measurements means that one measure some parameters and extract the properties sought by applying some type of theoretical model.

Ex: $R_{\text{tot}}, R(r) \rightarrow \mu_a, \mu_s'$

Inverse problem



The inverse problem is when you know the answer but not how to reach it!

Example in tissue optics:

You can measure diffuse reflectance, but what path did the photons take?

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Methods Available

- Steady state methods
 - Added-absorber
 - Fluence rate vs. distance from source
 - Steady-state diffuse reflectance
- Time-resolved methods
 - Time-resolved diffuse reflectance
 - Frequency-domain diffuse reflectance

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Steady State Diffusion

The steady state diffusion for a point source is

$$-\nabla^2 \mathbf{f}(\mathbf{r}) + \mathbf{m}_{eff}^2 \mathbf{f}(\mathbf{r}) = S(\mathbf{r})$$

This yields a solution for a infinite homogenous medium as:

$$\mathbf{f}(\mathbf{r}) = \mathbf{f}(\mathbf{r} = \mathbf{0}) \frac{1}{|\mathbf{r}|} \exp(-\mathbf{m}_{eff} \cdot |\mathbf{r}|) = \frac{P \mathbf{m}_{eff}^2}{4 \rho \mathbf{m}_a} \frac{1}{|\mathbf{r}|} \exp(-\mathbf{m}_{eff} \cdot |\mathbf{r}|)$$

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Solution to steady state diffusion

$$\mathbf{f}(\mathbf{r}) = \frac{P \mathbf{m}_{eff}^2}{4 \rho \mathbf{m}_a} \frac{1}{|\mathbf{r}|} \exp(-\mathbf{m}_{eff} \cdot |\mathbf{r}|)$$

where

$$\left\{ \begin{array}{l} \mathbf{m}_{eff} = \sqrt{3 \mathbf{m}_a (\mathbf{m}_a + \mathbf{m}_s (1 - g))} \\ \mathbf{m}_s' = \mathbf{m}_s (1 - g) \\ D = \frac{1}{3(\mathbf{m}_a + \mathbf{m}_s (1 - g))} = \frac{\mathbf{m}_a}{\mathbf{m}_{eff}^2} \end{array} \right.$$

Steady-state methods

- This means that it is primarily μ_{eff} that can be extracted from steady state diffusion from bulk tissue
- However, this is often what is required for light wavelengths obeying the diffusion approximation
- To be able to extract μ_a and μ_s' separately one need to measure more than the dependence of fluence rate vs. distance
- The g-value can never be evaluated with diffusion theory.

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Direct Fluence Rate Measurements

The most used technique to evaluate μ_{eff} from steady state measurements is to directly measure the fluence rate.

To do that one need to be inside the tissue ==> invasive measurements.

Need to measure light coming from all directions ==> diffusing fibre tips.

$$f(\mathbf{r}, t) = \int_{4\pi} L(\mathbf{r}, \mathbf{s}, t) d\omega$$

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Steady State Diffuse Reflectance

This method is an alternative, non-invasive way to measure the r-dependence of the fluence rate.

By measuring at a boundary, one need to take the boundary conditions into account.

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Calculate the steady state diffuse reflectance !

As an exercise, I would like that you derive an expression for the diffuse reflectance $R(\rho)$ of a semi-infinite highly scattering medium.

The fluence rate inside the medium can be written as:

$$f(r) = \frac{Pm_{eff}^2}{4pm_a} \left\{ \frac{\exp(-m_{eff} \cdot r_1)}{r_1} - \frac{\exp(-m_{eff} \cdot r_2)}{r_2} \right\}$$

$$\text{where } \begin{cases} r_1 = \sqrt{(z - z_0)^2 + \mathbf{r}^2} \\ r_2 = \sqrt{(z + z_0 + 2z_b)^2 + \mathbf{r}^2} \end{cases}$$

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Ex: Guidelines (I)

The diffuse reflectance is derived as the photon density current at $z = 0$ perpendicular to the surface:

$$R(\mathbf{r}) = h\mathbf{n}\mathbf{J}(\mathbf{r},0) \cdot \mathbf{n} = -D \frac{\mathbb{J}}{\mathbb{J}z} \mathbf{f}(\mathbf{r},z) \Big|_{z=0}$$

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Ex: Guidelines (II)

$$\mathbf{f} = \mathbf{f}_1 + \mathbf{f}_2$$

$$\frac{\mathbb{J}\mathbf{f}}{\mathbb{J}z} = \sum_i \frac{\mathbb{J}\mathbf{f}_i}{\mathbb{J}r_i} \frac{\mathbb{J}r_i}{\mathbb{J}z}$$

$$\frac{\mathbb{J}r_1}{\mathbb{J}z} \Big|_{z=0} = \frac{1}{2} \frac{1}{r_1} 2(z - z_0) = -\frac{z_0}{r_1}$$

$$\frac{\mathbb{J}\mathbf{f}_i}{\mathbb{J}r_i} = \left(-\mathbf{m}_{eff} - \frac{1}{r_i} \right) \mathbf{f}_i$$

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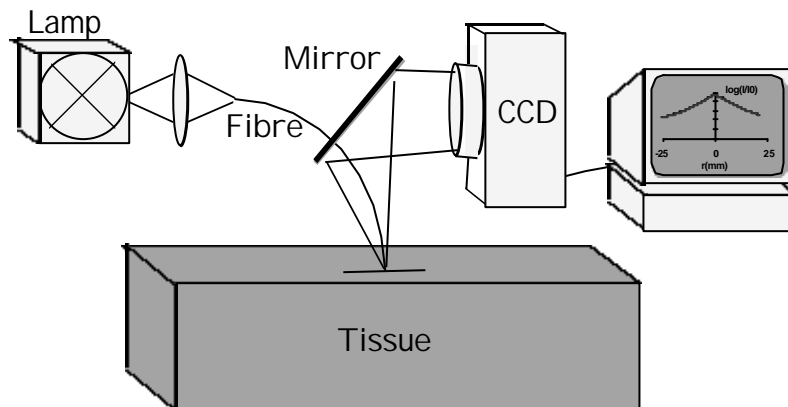
Diffuse reflectance equation

$$R(r) = \frac{1}{4p} \left[z_0 \left(m_{eff} + \frac{1}{r_1} \right) \frac{e^{-m_{eff} r_1}}{r_1^2} + (z_0 + 2z_b) \left(m_{eff} + \frac{1}{r_2} \right) \frac{e^{-m_{eff} r_2}}{r_2^2} \right]$$

- ➔ where r_1 is the distances from the real source,
- ➔ r_2 is the distance from the virtual source,
- ➔ z_0 is the distances between the real source and the real boundary,
- ➔ z_b is the distance between the real boundary and the extrapolated boundary,
- ➔ $2z_b + z_0$ is the distance between the real boundary and the virtual source.

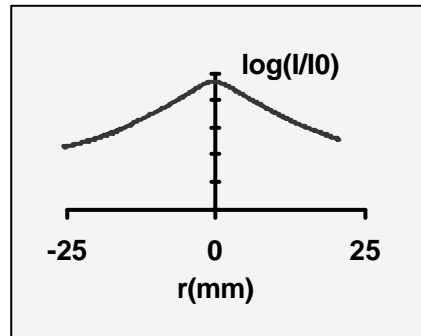
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Set-up for spatially resolved diffuse reflectance



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Diffuse Reflectance from Skin at 630 nm



Diffuse reflectance of normal skin irradiated with a pencil beam of light at 630 nm, measured as line across the irradiated spot.

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Added Absorber Method

Further another method that can be used to evaluate both μ_a and μ_s' is the so called added absorber method.

This method is destructive and can thus not be used *in vivo*. However, it is a very useful method for liquid tissue phantoms and for homogenised tissue.

The principle is to measure $\phi(r)$ vs. r , add some absorber and redo the measurements etc.

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Added Absorber Theory

The aim is to measure μ_{eff} for a number of added absorber concentrations.

$$m_{\text{eff}}^2 = 3m_a(m_a + m_s')$$

with some added absorption $m_a = m_{\text{at}} + m_{\text{ad}}$

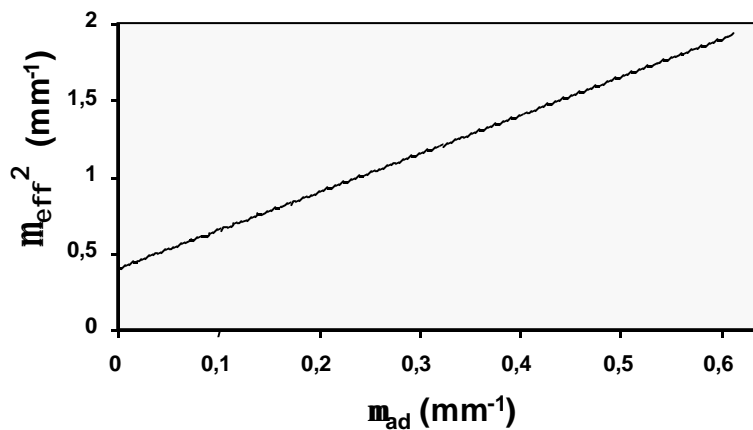
for the tissue and added dye, respectively. If

$$m_{\text{at}} + m_{\text{ad}} \ll m_s' \text{ then } m_{\text{eff}}^2 \approx 3(m_{\text{at}} + m_{\text{ad}})m_s'$$

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Added Absorber Plot

$$m_{\text{eff}}^2 = 3m_s'm_{\text{at}} + 3m_s'm_{\text{ad}}$$



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Time-resolved diffuse reflectance

The diffuse fluence rate in an infinite medium using a point source $\delta(r=0,t=0)$ can be expressed as:

$$f(\mathbf{r}, t) = c(4\mathbf{p}Dct)^{-3/2} \exp(-\mathbf{m}_d ct) \exp\left(-\frac{r^2}{4Dct}\right)$$

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Transform to frequency domain

The Fourier transform of this expression can be used to derive the solution for a modulated point source:

The fluence rate can be shown to be

$$S(\mathbf{r}, t) = \mathbf{d}(r = 0) \left\{ 1 + M_s e^{-i\omega t} \right\}$$

$$f(\mathbf{r}, t) = \frac{1}{4\mathbf{p}Dr} \left[e^{-r\sqrt{\frac{\mathbf{m}_d}{D}}} + M_s e^{\left[\frac{\mathbf{m}_d}{D} + i\frac{\omega}{Dc}\right]^{1/2}} e^{-i\omega t} \right]; \text{ with } \mathbf{m}_{df} = \sqrt{\frac{\mathbf{m}_d}{D}}$$

This means both a phase shift and a demodulation

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Diffusion equation in discrete form

The time resolved diffusion equation is

$$\frac{1}{c} \frac{\partial}{\partial t} \mathbf{f}(\mathbf{r}, t) - D \nabla^2 \mathbf{f}(\mathbf{r}, t) + \mathbf{m}_a \mathbf{f}(\mathbf{r}, t) = S(\mathbf{r}, t)$$

This can be rewritten in discrete form as

$$\frac{\mathbf{f}_x^{n+1} - \mathbf{f}_x^n}{\Delta t} = c' \frac{D}{2} \left[\frac{(\mathbf{f}_{x+1}^{n+1} - 2\mathbf{f}_x^{n+1} + \mathbf{f}_{x-1}^{n+1}) + (\mathbf{f}_{x+1}^n - 2\mathbf{f}_x^n + \mathbf{f}_{x-1}^n)}{(\Delta x)^2} \right] - c' \frac{\mathbf{m}_a}{2} (\mathbf{f}_x^n + \mathbf{f}_x^{n+1})$$

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